Original Research Article

Evaluation of shear bond strength of orthodontic resin and resin modified glass ionomer cement on bonding of metal and ceramic brackets

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Abstract

Objective: The aim of this study was to evaluate the shear bond strength of orthodontic resin and resin-modified glass ionomer cement on bonding of metal and ceramic brackets. Material and methods: Forty bovine teeth were sectioned and embedded into PVC with chemically-cured acrylic resin. The labial surfaces were flattened and received prophylaxis with pumice and water. Then they were divided into four groups, according to the bonding material and the type of bracket. Group 1: metallic bracket + Transbond XT; Group 2: metallic bracket + Vitremer; Group 3: ceramic bracket + Transbond XT; Group 4: ceramic bracket + Vitremer. The bonding was performed according to the manufacturers’ recommendations. The shear bond strength test was conducted in a universal testing machine (TIRAtest 2420) at a crosshead speed of 0.5 mm/min. Then, the fractured surfaces were evaluated using a stereomicroscope (×15 magnification) to check the adhesive remnant index. Data was subjected to two-way ANOVA and Tukey’s test for pairwise comparisons.
Results: The results suggested a non-significant effect of the interaction ($p > 0.97$), and only main factors were significant ($p = 0.0001$). The bond strength of Transbond XT was statistically higher than Vitremer. Ceramic brackets obtained the highest values of resistance when compared with metal brackets. Conclusion: The ceramic brackets bonded with Transbond XT orthodontic resin have excellent bond strength results.

Introduction

The dental advanced has stimulated numerous researches aiming to analyze different adhesive materials which could be used in orthodontic brackets bonding to tooth enamel. Additionally, it is of fundamental importance that the material present an effective bonding to tooth surface, resisting to masticatory and orthodontic forces constantly applied. However, it is necessary that the material also enable an easy removal without damaging the enamel [5, 7, 10, 13, 18, 21].

The first reports on direct bonding of brackets to enamel surface, according to literature, was conducted by Sadler in 1958, and initially the bracket bonding was performed through orthodontic bands on all teeth. In 1977, Zachrisson [27] described numerous disadvantages of this procedure: difficulty of performing oral hygiene, larger chairtime, and poor aesthetics. Therefore, direct bonding technique of orthodontic brackets was an indispensable advancement for treatment developing and simplification. However, this technique was only possible because of the etching of tooth enamel, described by Buonocore in 1955 [4], resulting in a routine treatment in daily practice. Attempting to facilitate the procedures during orthodontic bonding, the manufacturers have developed materials promising efficacy and aiming to decrease the number of clinical steps and to meet the demand on aesthetics and comfort [5, 6, 9, 18]. The association of the etching of enamel surface with Bis-GMA-based composite resins has been, since the 80s, the bonding method of choice and the scope of several studies because this association presents clinically satisfactory bond strength and dimensional stability [10, 15, 16, 19].

Glass ionomer cement and compomer materials have been evaluated and available on dental market for performing the bonding of orthodontic brackets because they show the single feature of fluoride releasing; this is capable of preventing caries lesions around orthodontic brackets and bands after the treatment ending as well as of enabling the chemical adhesion to tooth structure, not necessitating previous enamel etching [5, 13, 17, 21, 26].

Orthodontic brackets may be composed of several materials, such as stainless steel, polymers, porcelain, titanium or their combination. Ceramic brackets have been available for clinical use since 1987. They were designed to combine its excellent aesthetics with the well-known reliability of stainless steel brackets. However, a greater risk of enamel fracture during bracket debonding has limited its use [1, 2, 7, 25].

The current need of testing the numerous materials used to bond orthodontic brackets justifies this present study, whose aim was to analyze and compare in vitro the shear bond strength of two different materials (Transbond XT resin cement and Vitremer resin-modified glass ionomer cement) for the bonding of metallic and ceramic orthodontic brackets as well as to evaluate the enamel conditions after the debonding, through adhesive remnant index (ARI).

Material and methods

Forty sound mandibular incisor teeth were selected. The teeth were cleaned and stored in a plastic recipient with distilled water under refrigeration, at 6°C until their use [22].

The study was based on the methodology established by the International Organization for Standardization (ISO), specification TR11405 for mechanical bond strength tests [11].

The root portion was sectioned with aid of carborundum discs, mounted in straight handpiece (Dabi Atlante, Ribeirão Preto, São Paulo, Brazil), at low speed, under refrigeration, at 1 cm shorter of the incisal edge. Tooth blocks were embedded in chemically-cured resin (Clássico Artigos Odontológicos, São Paulo, Brazil) within PVC tubes.

With the aid of a horizontal polishing machine (Aropol 2V, Arotec, Cotia, São Paulo, Brazil) and
sandpapers in descending order #120, #220, #400 and #600 (3M, Sumaré, São Paulo, Brazil), the enamel surface was flattened under refrigeration.

Prior to bonding, tooth surfaces underwent dental prophylaxis with Robinson brush (Microdont, São Paulo, Brazil) mounted in contra-angle handpiece (Dabi Atlante, Ribeirão Preto, São Paulo, Brazil), at low speed, and superfine pumice (SS White, Rio de Janeiro, Brazil) and water for 10 seconds. Following the surfaces were washed by water/air spray for 10 seconds and dried by air jet.

At this stage of the study, the samples were randomly divided into four groups (n = 10), according to the bonding material and the bracket type. The brackets used were Roth type for maxillary right central incisor, with bracket base design of 12.03 mm².

Group 1 was composed by metallic brackets (3M Unitek, Monrovia, California, USA) + Transbond XT; group 2 was composed by metallic bracket + Vitremer resin-modified glass ionomer cement; group 3 was composed by ceramic brackets (3M Unitek, Monrovia, California, USA) + Transbond XT; and group 4 was composed by ceramic brackets + Vitremer resin-modified glass ionomer cement (table I). The sequence used for bonding technique is described below:

- Groups 1 and 3: enamel etching with 37% phosphoric acid for 15 seconds, washing and drying for the same time, application of XT primer, brackets bonding with Transbond XT resin, removal of the excesses through dental probe, light-curing for 40 seconds: 10 seconds at each tooth surface (mesial, distal, incisal and gingival) at a distance of 1 mm from the bracket;
- Groups 2 and 4: application of Vitremer primer for 30 seconds on tooth surface, drying of the primer with air jet for 15 seconds, light-curing for 20 seconds, mixing of the powder and liquid for until 45 seconds, brackets bonding with the cement, removal of the excesses with dental probe, light-curing for 40 seconds: 10 seconds (mesial, distal, incisal and gingival) at a distance of 1 mm from the bracket.

Light-curing was accomplished by using Ultralux (Dabi Atlante, Ribeirão Preto, São Paulo, Brazil), a device composed of halogen light of mean intensity of 400 mW/cm².

<table>
<thead>
<tr>
<th>Material</th>
<th>Constituents (batch number)</th>
<th>Chemical composition</th>
<th>Manufacturer</th>
</tr>
</thead>
<tbody>
<tr>
<td>Transbond XT</td>
<td>Primer (9FR 2012-03)</td>
<td>Triethylenoglycol-dimethacrilate, Bis GMA</td>
<td>3M Unitek Monrovia, California, USA</td>
</tr>
<tr>
<td></td>
<td>Adhesive paste (9hg 2012-05)</td>
<td>Silica, BIS-GMA, Silane, N-dimethyl benzocaine, hexa-fluoro-phosphate</td>
<td></td>
</tr>
<tr>
<td>Vitremer</td>
<td>Primer (9CJ 2012-03)</td>
<td>Copolymer of modified polyacrylic acid, methacrylate groups, ethanol, camphorquinone</td>
<td>3M ESPE, Seefeld, Germany</td>
</tr>
<tr>
<td></td>
<td>Powder (9TJ 2012-04)</td>
<td>Fluoro-aluminosilicate, potassium persulfate, ascorbic acid and pigments</td>
<td></td>
</tr>
<tr>
<td></td>
<td>Liquid (9JH 2012-04)</td>
<td>Polialcenoic acid, methacrylate groups, water, HEMA, camphorquinone</td>
<td></td>
</tr>
</tbody>
</table>

*Manufacturers’ information

After bonding, the samples were kept into distilled water at 37±2°C for 24 hours. Next, to perform the test, the bonded bracket was involved by a hook made of metallic orthodontic wire (Morelli Ortodontia, Sorocaba, São Paulo, Brazil) with 0.6 mm thickness [7, 23], through load cell of 500 N in a universal testing machine (TIRA/mach 2420, TIRA Maschinenbau GmbH, Schalkau, Germany), at crosshead speed of 0.5 mm/min.
Shear bond strength values were obtained in Newtons (N), which were next calculated in MegaPascals (MPa). The shear bond stress was calculated by using the load applied through the formula \( S = \frac{F}{A} \), in which \( S \) = shear bond strength, \( F \) = load (N) required for the disruption of the bracket/tooth union and \( A \) = area of bracket base (mm²).

Bond strength data were submitted to two-way ANOVA (bond material X bracket type ) and Tukey test for means contrast at \( \alpha = 0.05 \).

After the trial, each fractured surface of the samples was evaluated by using stereomicroscope (Quimis Q7355–TZ, Diadema, São Paulo, Brazil), at x15 magnification, to quantify the adhesive remnant index (ARI).

### Results

Shear bond strength values of the tested groups are seen in table II. The analysis of variance showed that the interaction of the factors was not significant \( (p > 0.97) \), only the main factors were statistically significant \( (p = 0.0001) \).

Transbond XT \( (8.2 \pm 3.7 \text{ MPa}) \) showed the highest shear bond values when compared to Vitremer \( (5.5 \pm 3.2 \text{ MPa}) \). The ceramic bracket \( (8.3 \pm 2.9 \text{ MPa}) \) obtained shear bond strength values higher than metallic brackets \( (5.4 \pm 3.9 \text{ MPa}) \).

### Table II – Means and standard deviations of the shear bond strength (MPa) of the tested groups

<table>
<thead>
<tr>
<th>Bracket type</th>
<th>Bonding material</th>
<th>Transbond XT</th>
<th>Vitremer</th>
<th>Total</th>
</tr>
</thead>
<tbody>
<tr>
<td>Metallic</td>
<td></td>
<td>6.8 ± 3.6</td>
<td>4.0 ± 3.2</td>
<td>5.4 ± 3.9(^b)</td>
</tr>
<tr>
<td>Ceramic</td>
<td></td>
<td>9.6 ± 2.6</td>
<td>6.9 ± 2.7</td>
<td>8.3 ± 2.9(^a)</td>
</tr>
<tr>
<td><strong>Total</strong></td>
<td></td>
<td><strong>8.2 ± 3.7(^a)</strong></td>
<td><strong>5.5 ± 3.2(^b)</strong></td>
<td>-------</td>
</tr>
</tbody>
</table>

\(^a\) Different letters indicate statistically significant differences \((p < 0.05)\).

The assessment of ARI scores met the criteria idealized by Årtun and Bergland in 1984 \[3\]: 0 – none amount of composite adhered to the enamel; 1 – less than half of the composite adhered to the enamel; 2 – more than half of the composite adhered to enamel; and 3 – all composite adhered to enamel, including impression of the bracket net.

At this stage, we did not apply any statistical test; only the frequency of each index in each group was evaluated. In the assessment of ARI, the scores were observed within each group (table III).

### Discussion

Bracket bonding to enamel has been a critical issue in Orthodontics since the direct bonding introduction, where is extremely important the biomechanical stability of the bracket/adhesive interface which transfers the force generated by the archwires activation to the tooth \[10\]. The occurrence of accidental debonding of brackets is a frustrating aspect inherent to orthodontic practice, resulting in treatment time increase. A good orthodontic treatment path is mandatory for malocclusion correction, and therefore, the use of safer and more reliable materials is always desirable \[7\].

Bracket bonding has been the scope of several studies evaluating its bond strength aiming to improve the adhesive systems for orthodontic purposes \[8, 10, 13\].

The bonding of materials to enamel has been studied by several researchers, indicating that this type of substrate for shear bond strength testing \[6, 7, 8, 12, 15, 17, 18, 19, 20\]. The use of bovine teeth by this study was motivated by the studies of Nakamichi et al. \[14\], who in 1983 studied the possibility of substituting human teeth in adhesion tests.
Because bovine tooth surfaces are very irregular, making difficulty the bonding of metallic brackets to the straight base of the metallic brackets, we opted by the flattening of the bovine tooth enamel to standardize the surface to be bonded; this allowed that at the moment of brackets bonding, the cement agents show a thickness as equal as possible [7, 8, 12, 14, 19].

Although dental market displays different types of brackets made of different materials, we chose stainless steel because they are the most used brackets in clinical practice [15, 16, 17, 19, 20], and ceramic brackets because of the increasing aesthetic demand of orthodontic patients [1, 2, 7, 25].

The combination of 37% phosphoric acid and Transbond XT was the protocol selected by control group because of its efficacy and excellent values obtained when tested with other bonding materials [1, 2, 8, 10, 11, 15, 16, 17, 18, 25, 26].

Resin-modified glass ionomer cements (RMGICs) showed a shear bond strength value smaller than the resin material. Based on these results, one may assume that the low bond strength of Vitremer was probably because of the manufacturer's recommendation of not performing enamel etching. The lack of microporosities on the substrate jeopardizes the formation of the mechanical bond between the enamel and Vitremer; therefore, bonding occurs only through chemical bond which should resist to mechanical efforts [5]. Another reason may be the low cohesive resistance of the ionomer materials.

On the other hand, this low cohesive resistance may be beneficial because it may cause lesser damage to enamel surface than phosphoric acid etching, during debonding. This is because the highest pH of polyacrylic acid than phosphoric acid. This lower bond strength of RMGICs could constitute an advantage, once it facilitates the removal of the bonding material's remnants during enamel finishing and polishing; however, this may lead to the early debonding of the brackets, interfering in the treatment prognosis.

Despite of the fact that glass ionomer cements reduce the biochemical problem of caries lesions provoked by poor oral hygiene and their improvement regarding physical properties, doubts are still raised regarding the advantages of their use in brackets bonding [17, 23].

According to the results of this present study, there were statistically significant differences between the bracket's materials. The mean shear bond strength was always higher for ceramic than for metallic brackets. This can be attributed to the more effective light-curing in ceramic brackets because of their translucence, enabling greater light transmission to the bonding material and also because of the materials compatibility. Concerning to metallic brackets, incomplete light-curing of the bonding material could have happened below the bracket's base because this material does not allow the correct light passage. According to Al-Saleh and El-Mowafy (2010) [2], even if greater time amounts were used, the authors did not reach a satisfactory light-curing.

Due to these aforementioned reasons, the results found by this present study are in agreement with numerous studies demonstrating that ceramic brackets show the highest bond strength values when compared with metallic brackets [1, 2, 7, 25].

Concerning to the adhesive remnant index (ARI), in groups 1 and 3 (Transbond XT), the most found score was 3, showing that most of the fractures after debonding occurred at the composite bracket interface and indicating the efficient bonding of the material to tooth substrate. On the other hand, in groups 2 and 4 (Vitremer), the most found scores were 0 and 1, indicating an unsatisfactory bonding of the material to tooth substrate.

These results are in agreement with many studies in literature, in which cohesive fractures occurred within the composite, that is, the material remains bonded to the enamel surface and consequently preventing the enamel from eventual traumas [8, 15, 16, 20, 21, 25]. This seems to be the fracture interface most favorable for a safe debonding because it demonstrates that the enamel's cohesive force was higher than the bonding force between the bracket base and the adhesive. Therefore, the occurrence of enamel fractures is practically inexistent, and the removal of the residual adhesive is executed with the aid of specific burs which do not damage the tooth tissue [7, 19].

ARI results showed by this study is of great interest because it enables the orthodontist to choose better materials presenting clinical responses with greater adhesive remnant on tooth surface after bracket debonding, which may be safer, avoiding enamel fractures and maintaining the tooth's integrity [16].

Conclusion

Considering this study's methodology and results, it can be concluded that the ceramic bracket bonded with the orthodontic resin Transbond XT showed excellent shear bond strength results.
References


